

POLITECNICO **MILANO 1863**

INTRODUCTION

- Predicting flow patterns in nasal cavities by CFD can provide essential information on the relationship between patient-specific geometrical characteristics and health problems.
- Understanding must improve further for CFD to become a reliable tool in clinical use.

RESULTS

General trend

LES, steady inspiration:



Separation below larynx

2. LES or DNS?



3. Differences









Strong laryngeal jet





RANS/LES/DNS SIMULATIONS OF THE AIRFLOW IN NASAL CAVITIES

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OBJECTIVES

Evaluate the effect of:

- 1. RANS/LES models
- 2. Boundary conditions
- 3. Numerical schemes





Main pressure drop at larynx

• $\nu = 1.45 \cdot 10^{-5} \, \mathrm{m}^2 / \mathrm{s}$ • $\nu_{sqs} < \nu$

 \Rightarrow LES works as DNS





MATERIALS & METHODS

1. Geometry: • Carefully selected anatomy • External boundary moved away • Paranasal sinuses included from the nostrils • Section 10 is critical: inlet during 2. Mesh: inspiration and outlet during expi-• Number of cells 7M ration • 6 near-wall layers • Two tests: $p_{tot} = p + \frac{1}{2}\rho |\mathbf{U}|^2$ and con-• y^+ first cell between 4 and 5 stant velocity realized with a fringe region with body forces. 4. Solver: OpenFOAM finite volume method • RANS: – $k - \omega SST$ turbulence model – SimpleFoam steady incompressible solver • LES: Smagorinsky turbulence model

CONCLUSION & FUTURE RESEARCH

- Once a suitable boundary condition is found its effect on the solution is small. • High influence of numerical schemes. Difficult to find a steady second order solution with RANS equations.
- Large difference between RANS and LES simulations, mainly at the nasopharynx.

Future work:

• Ongoing *Particle Image Velocimetry* to validate CFD. • Unsteady breathing cycle.

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3. Boundary conditions at inlet/outlet:

- PimpleFoam unsteady incompressible solver
- $\mathbf{U}_{\mathbf{Mean}} = \sum_{i=1}^{n} \frac{1}{N} \mathbf{U}_{\mathbf{i}}$

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